

1     **ADVANCES IN THE USE OF MICROFOCUSED ULTRASOUND FOR FACIAL**  
2                                   **REJUVENATION**

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5     **Abstract**

6     The demand for non-invasive technologies to address facial rejuvenation and  
7     achieve a lifting effect has increased significantly over the past decades. Micro-  
8     focused ultrasound is a technology capable of inducing microthermal lesions at  
9     varying tissue depths, including the superficial musculoaponeurotic system  
10    (SMAS) and the dermis. Following the formation of these lesions, determined  
11    by power adjustment and the precise delivery of concentrated energy across  
12    different layers, a healing process is initiated, ultimately leading to SMAS  
13    contraction and dermal restoration, primarily associated with collagen  
14    synthesis. Accordingly, this study aimed to evaluate an application strategy  
15    utilizing micro-focused ultrasound on the facial region and to assess the  
16    outcomes resulting from this therapeutic approach. The findings demonstrated  
17    improved tissue support, particularly in the subocular region, temples, and  
18    nasolabial fold. Thus, it can be concluded that the use of micro-focused  
19    ultrasound on the facial region is a safe and effective therapeutic approach for  
20    treating skin aging, as it enhances tissue support and restores the tissue matrix,  
21    which also contributes to improved skin laxity.

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28    **Keywords:** rejuvenation, ultrasound, skin regeneration, dermal matrix

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## 38 INTRODUCTION

39 The skin aging process is multifactorial, affecting all skin layers and  
40 resulting in a significant degradation of collagen, a key structural component of  
41 the dermal matrix. The loss of intrinsic structural components results in the  
42 appearance of wrinkles and expression lines, often accompanied by local laxity,  
43 factors that directly impact the aesthetic appearance and overall quality of life  
44 of individuals. Notably, several other factors contribute to the onset and  
45 progression of this process, including hormonal influences, lifestyle habits,  
46 dietary behaviors, and external factors such as prolonged exposure to UVA and  
47 UVB radiation (1,2).

48 Currently, there is a growing preference for non-invasive techniques that  
49 achieve comparable rejuvenation effects while minimizing post-procedural  
50 downtime. As a result, continuous technological advancements are being  
51 developed to meet the increasing demand in this sector. Among the available  
52 technologies, micro-focused ultrasound has demonstrated remarkable progress  
53 in both development and clinical application (3–5).

54 This technology relies on the emission of ultrasound-generated  
55 mechanical waves that are precisely focused on specific points with high energy  
56 concentration, allowing for penetration at different depths. The technological  
57 design that enables this precision consists of a carefully engineered metallic  
58 structure with an exact concavity, ensuring the mechanical wave is directed to a  
59 single focal point with mathematically calibrated penetration depth. The  
60 treatment depth is determined by the targeted skin layers, utilizing spacers  
61 calibrated at 4.5 mm, 3.0 mm, and 1.5 mm to safely reach from the superficial  
62 musculoaponeurotic system (SMAS) down to the papillary dermis (6–12).

63 Due to the high-energy concentration delivered to a precise focal point,  
64 the resulting biological effect is thermal damage. Therefore, treatment protocols  
65 must account for the target area size and the number of pulses applied.  
66 Additionally, the quality of the treated tissue influences the outcome, as  
67 effective healing is essential to sustain the lifting effect observed immediately  
68 after treatment. The healing process associated with this type of lesion involves  
69 localized inflammation and biochemical signaling of factors responsible for cell  
70 differentiation and proliferation, with the most notable event being collagen  
71 synthesis, which contributes to the formation of a new tissue matrix (13,14).

72 Clinically, this treatment is advantageous as it is safe, effective, painless,  
73 and free from significant adverse effects, since only internal tissue layers are

74 targeted, leaving the outer skin surface unaffected. However, despite extensive  
75 literature on the subject, gaps remain regarding the optimal application  
76 methodology.

77 Some strategies are based on linear application, dictated by the emission mode  
78 of certain devices, whereas advancements in modern applicators allow  
79 practitioners greater flexibility to align treatment with muscle fiber direction  
80 and the SMAS, thereby enhancing the lifting effect.

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## 82 TECHNOLOGICAL EVOLUTION

83 Micro-focused ultrasound technology aims to emit targeted energy at  
84 single points capable of producing a thermal microlesion in the target tissue.  
85 Some equipment has an electronic form of emitting this energy, in lines, but  
86 requires cartridges that have a limited number of shots because the half-life of  
87 the crystal is compromised. This condition results in additional equipment costs  
88 that will result in added value in the therapeutic protocol. Currently, innovation  
89 in the development of micro-focused ultrasound equipment allows the  
90 production of this energy emission at no additional cost and without shot  
91 limits, in addition to preserving the half-life of the piezoelectric crystal that  
92 maintains the quality of the equipment for life, without the need for frequent  
93 replacements as presented by VISAGE® equipment, developed, and  
94 manufactured by the Brazilian Medical Equipment Industry – IBRAMED  
95 (Figure 1).

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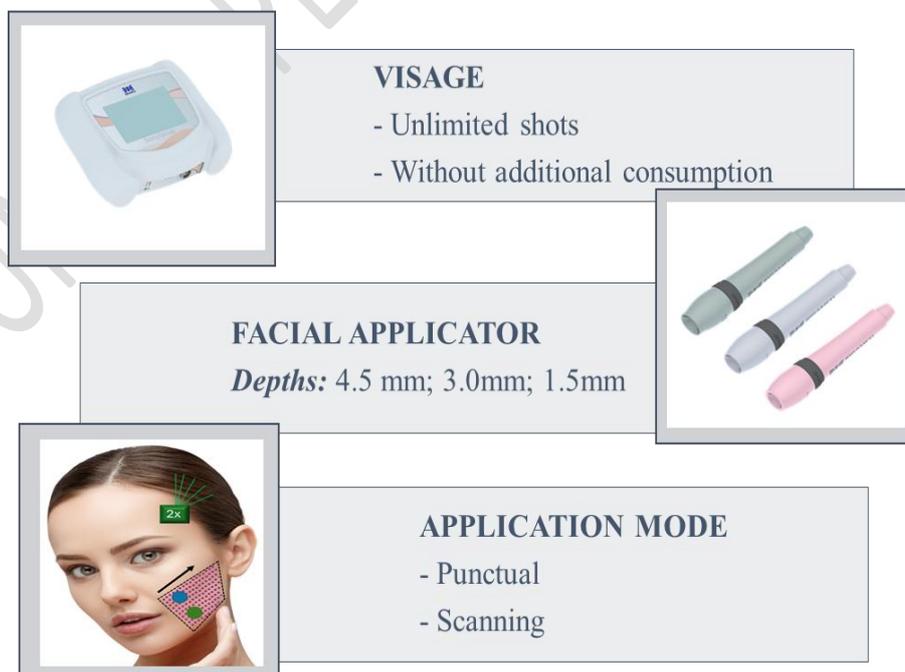
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111 *Figure 1 - Technological characteristics of VISAGE® equipment*

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113 With this equipment it is possible to achieve different depths in the target  
114 tissue. In the case of this study, was used three types of applications, with  
115 distance of 4.5, 3.0 and 1.5 mm, which can deliver the energy of interest, from  
116 the layer of the musculoaponeurotic system (SMAS) to the layer of the papillary  
117 and reticular dermis, considered more superficial (Figure 2). The emission of  
118 punctual energy, in this case, comes from a metal concavity present in the tip of  
119 the applicator, which allows the correct direction of this heat in the tissue layers,  
120 with the entire process only being possible due to precise mathematical  
121 calculations. In addition, the equipment offers therapeutic advantages through  
122 the possibility of different emission modes, punctual or scanning, associated  
123 with the therapist's freedom of choice for application in lines or even in circular  
124 movements, aiming in this case at tissue anchoring methods. With technological  
125 innovation and the autonomy of the professional regarding the application  
126 strategy, new and interesting therapeutic approaches emerge that benefit from  
127 microfocused ultrasound and expand to different areas that target facial  
128 treatment.

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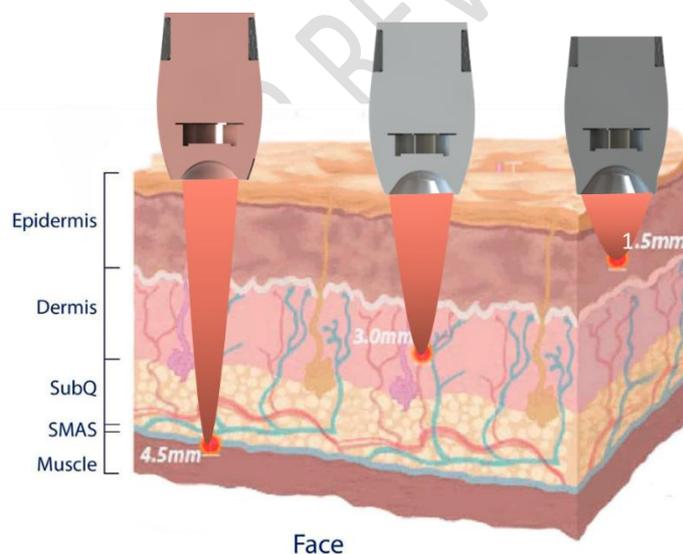
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139 *Figure 2 - Demonstration of the depth of action in the target tissue for each applicator*

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141 **METHODOLOGY**



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142 **Type and Location of Research**

143 This case study was conducted at Casal da Beleza Clinic – Personalized  
144 Aesthetics in collaboration with the Research Group of Brazilian medical  
145 equipment industry – IBRAMED.

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147 **Clinical Protocol**

148 The protocol application adhered to the safety guidelines provided by  
149 the manufacturer, considering the demarcated areas illustrated in Figures 1 and  
150 2. Both application modes available in the equipment—point mode and  
151 scanning mode—were utilized for this protocol. Additionally, three spacers  
152 measuring 4.5 mm, 3.0 mm, and 1.5 mm were employed to target tissue layers  
153 ranging from the SMAS to the superficial dermis. As the protocol aimed to  
154 achieve a lifting effect followed by rejuvenation, the therapeutic strategy began  
155 with point mode application using 4.5 mm and 3.0 mm spacers on the midface  
156 region. This was followed by scanning mode application using all three spacers  
157 in the same area, as shown in Figure 1. The parameters used for this application  
158 are detailed in Figure 1. For treatment of the frontal and temporal regions, as  
159 illustrated in Figure 1, 4.5 mm and 3.0 mm spacers were used, always starting  
160 with the deeper one. Both point and scanning application modes were  
161 employed, following the previously described parameters. To complete the  
162 protocol, the 1.5 mm spacer was used in scanning mode exclusively on the  
163 midface region. Additionally, this 1.5 mm spacer was applied to other facial  
164 areas, as demonstrated in Figure 2, using the same energy settings but with  
165 reduced application time and number of pulses. It is important to highlight that  
166 Figure 2 provides a detailed representation of the appropriate treatment regions  
167 while also indicating risk areas.

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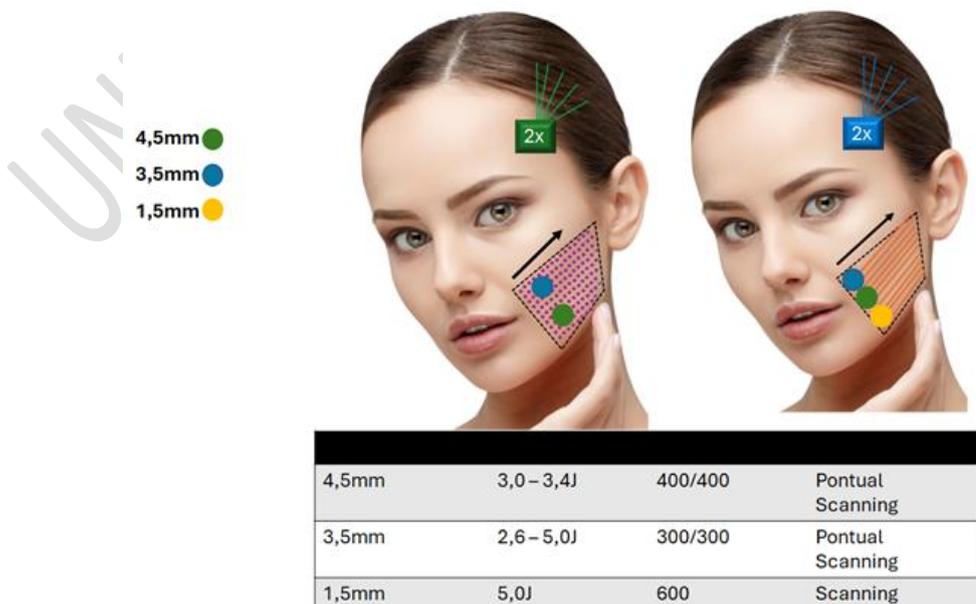
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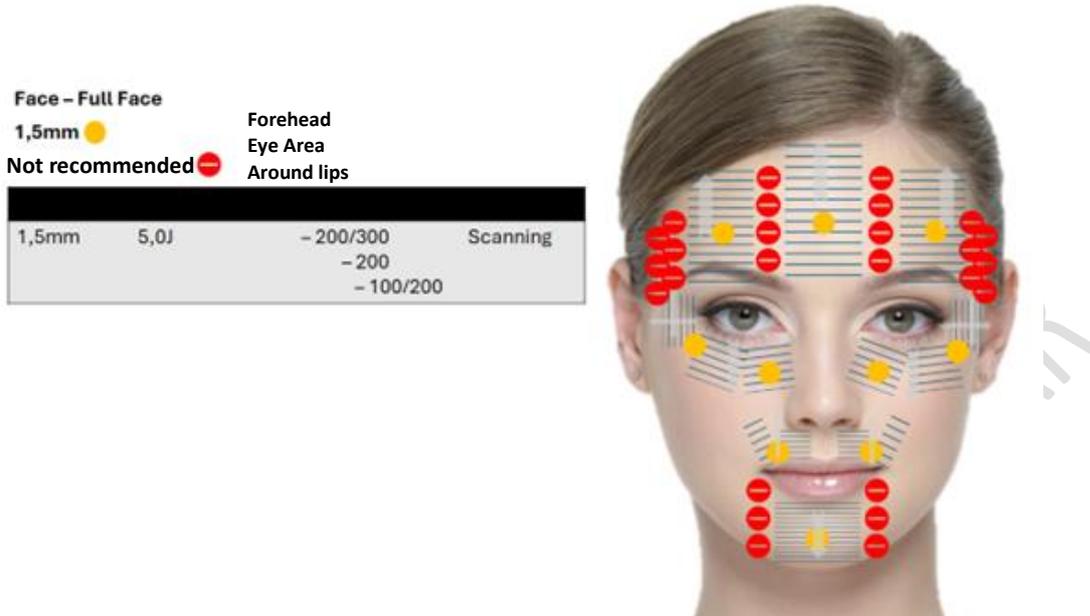
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180 Figure 3 - Areas and application modes considering the three target distances

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183 Figure 4 -Application areas considering only the surface layer

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## 185 CLINICAL EVALUATION

### 186 Anamnesis of the Treatment Area

187 During evaluations, an anamnesis form designed specifically for this  
188 study will be completed. This form will include personal information, lifestyle  
189 habits, medications, observations related to the inspection of the treatment area,  
190 history of aesthetic procedures performed in the area, skin phototype, and a  
191 patient satisfaction questionnaire regarding the treated region.

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### 193 Photographic Analysis

194 For photographic documentation, a digital camera will be used with the  
195 patient in an upright position. The assessment will focus on the central and  
196 lateral regions of the face in a neutral expression. The patient will maintain an  
197 upright posture, with their gaze aligned with the horizon and head centered in  
198 relation to the camera's positioning. The camera will be placed at 90 cm from  
199 the patient, with the zoom set to 1x.

200

### 201 Assessment of Skin Appearance

202 Improvement in the appearance of photoaged skin will be assessed using  
203 the GAIS (Global Aesthetic Improvement Scale), where: 0 = no improvement, 1

204 = slight improvement, 2 = moderate improvement, 3 = marked improvement,  
205 and 4 = significant improvement.

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### 207 **Patient Tolerance to Treatment**

208 Pain perception in the treated area was evaluated using a subjective 0–10  
209 visual analog scale, where: 0 = no pain or warmth, 1–4 = mild pain or warmth,  
210 5–7 = moderate pain or warmth, and 8–10 = intense pain or warmth.

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### 212 **Patient Satisfaction Assessment**

213 Participant satisfaction regarding treatment results and comfort in the  
214 treated area was assessed using a subjective 1–5 scale, where: 1 = very  
215 dissatisfied/very uncomfortable, 2 = dissatisfied/uncomfortable, 3 = no  
216 difference/no opinion, 4 = satisfied/comfortable, 5 = very satisfied/very  
217 comfortable (Noyman et al., 2021).

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## 219 **RESULTS**

220 Photographic analysis demonstrated improvements in skin texture and  
221 quality. Overall, an increase in tissue support was observed, which resulted in a  
222 softening of the nasolabial fold and deep wrinkles in the forehead region.  
223 Additionally, a significant improvement was noted in the upper eyelid, likely  
224 due to treatment applied to the area between the frontal and temporal bones,  
225 extending into the scalp. Another area that benefited from this application was  
226 the upper eyelids and the fine wrinkles around the lateral eye region.  
227 Regarding tissue vitality, the entire face exhibited visible improvement, with  
228 particular emphasis on the midface and subocular regions, which clinically  
229 translated into a rejuvenated appearance and a reduction in laxity — commonly  
230 associated with a tired look.

231 Based on the skin improvement scale, as rated by an average of three  
232 blinded evaluators, the treatment outcome was classified as 3, indicating a  
233 marked improvement. For pain tolerance, assessed during the procedure, the  
234 patient rated their experience as 4, corresponding to mild pain and warmth.  
235 Thirty days post-treatment, the patient satisfaction scale was applied, yielding a  
236 score of 4, indicating overall satisfaction with the results.

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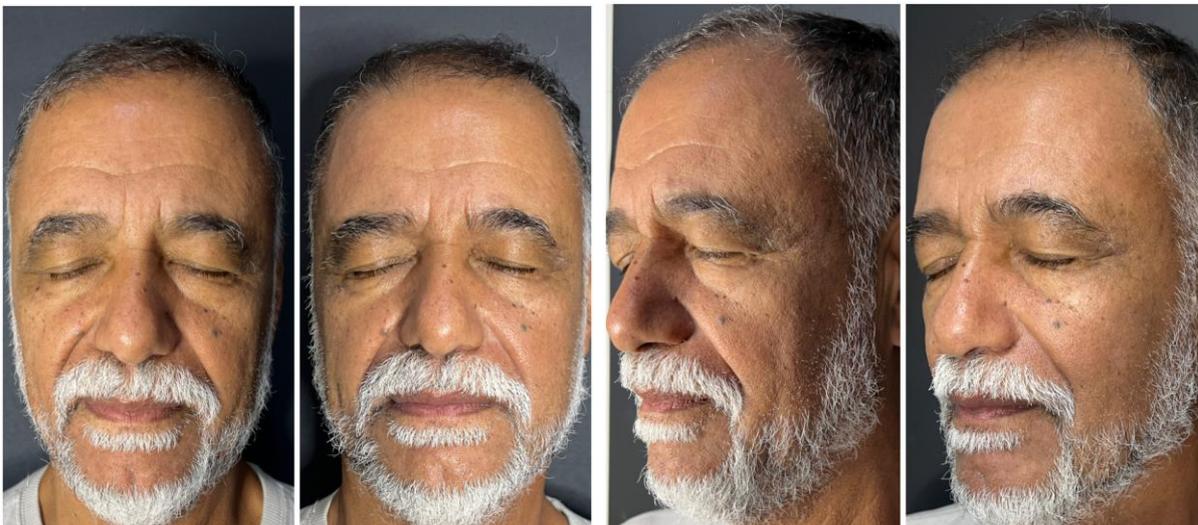
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## 246 **DISCUSSION**

247 Microfocused ultrasound technology has emerged as an effective  
248 alternative for restoring the dermal matrix, thereby addressing clinical concerns  
249 related to skin rejuvenation and laxity. Beyond these benefits, it offers a distinct  
250 advantage over other technologies due to its ability to target the Superficial  
251 Musculoaponeurotic System (SMAS), leading to significant tissue contraction  
252 that results in a lifting effect. Given these characteristics and its biological  
253 mechanism, thermal-induced coagulative microinjury, this technology is  
254 applicable to various body areas. These indications have been well-documented  
255 in scientific studies that confirm both its efficacy and safety (15–19). Despite the  
256 established effects, there remains no consensus regarding the optimal  
257 application methods. Some devices administer pulses electronically, allowing  
258 for application solely along linear patterns, whereas more versatile systems  
259 offer both point-by-point and scanning modes, with the method of application  
260 determined based on the desired clinical outcome. Thus, the objective of this  
261 study was to evaluate the effects of microfocused ultrasound using point-by-  
262 point and scanning application modes as part of a therapeutic strategy for  
263 treating age-related facial changes.

264 The results revealed notable improvements in facial tissue support. In the  
265 forehead and eyebrow regions, an observable lifting effect was achieved  
266 through structural reinforcement, contributing to an enhanced appearance of  
267 the eyelids and overall facial elevation. These aspects were evaluated and  
268 confirmed by Alam et al.,(20), which reported that after a single application of  
269 microfocused ultrasound to the forehead region, an elevation of up to 1.9 mm in  
270 the eyebrow area on both sides was observed in more than 83% of treated  
271 patients, with this effect being maintained for three months after the procedure.

272 Microfocused ultrasound energy possesses distinct properties that  
273 promote tissue support by replenishing the dermal matrix. This is directly  
274 linked to its ability to deliver targeted energy at varying depths. In the case of  
275 treatment in deeper layers, such as the SMAS, it becomes evident that the  
276 induced microinjury results in facial lifting, with a significant improvement in  
277 overall muscle support, which greatly enhances the appearance of the final  
278 outcome. At shallower depths, the treatment targets the papillary and reticular  
279 dermis, primarily stimulating dermal regeneration and collagen synthesis. This  
280 process not only reinforces tissue structure but also enhances skin elasticity,  
281 hydration, and overall vitality (21).

282 Technologies aimed at improving facial laxity and tissue support, such as  
283 lasers and radiofrequency, are well-established in the literature. However, due

284 to the unique cellular mechanisms of microfocused ultrasound — which induce a  
285 robust tissue repair process leading to significant improvements in fine lines  
286 and skin laxity—this technology is gaining recognition as a non-invasive and  
287 painless alternative in aesthetic treatments (9,22).

288 The primary mechanism of action of microfocused ultrasound involves  
289 the precise and intense delivery of energy within a short duration (20–50  
290 milliseconds), reaching various depths and effectively inducing thermal  
291 microinjuries in three key layers: the musculoaponeurotic layer, papillary  
292 dermis, and reticular dermis, at approximately 5 mm depth. Once these  
293 microlesions are established, the tissue repair process initiates, progressing  
294 through inflammation, proliferation, and remodeling phases, with the primary  
295 objective of dermal reconstruction via collagen synthesis. As it is a treatment  
296 that induces internal lesions, it has the advantage of not causing changes to the  
297 epidermis. Therefore, the patient does not require special care after the  
298 application, and no morphological changes, irritability, or erythema are visible  
299 in the superficial layer (9,20,22,23).

300 A study by Ko et al.(24) confirmed that microfocused ultrasound is safe  
301 and effective for enhancing facial elasticity and contouring. Park et al.  
302 concluded that microfocused ultrasound is a promising tool for addressing fine  
303 lines and skin laxity in the facial region of Asian patients, demonstrating,  
304 through an evaluation scale, a significant improvement three months after  
305 treatment, with its efficacy maintained for up to six months, particularly in the  
306 jowls, cheeks, and perioral area. Vachiramou et al. (15), evaluated the use of  
307 microfocused ultrasound for pore reduction in the facial region and found the  
308 technology to be effective, with high patient satisfaction. Friedman et al. (2)  
309 reported positive results in improving laxity in the submental and neck regions.  
310 However, the authors noted that achieving the desired clinical outcomes  
311 requires patients to present with only mild skin laxity. Regarding the longevity  
312 of the results (25), it is emphasized that this may be associated with the  
313 expression of the HSP47 protein, responsible for the quality of collagen  
314 crosslinking.

315 In a review conducted by Contini et al., the authors concluded that the  
316 technology is effective for treating clinical conditions classified as mild to  
317 moderate skin laxity, and that just one treatment session can result in long-term  
318 improvement. These findings align with the outcomes of the clinical case  
319 presented in this study, which demonstrated significant changes after one  
320 month of treatment. Considering the above, we conclude that microfocused  
321 ultrasound is effective in promoting facial rejuvenation, with notable  
322 improvement primarily in the subocular region, nasolabial folds, and temples,  
323 thereby enabling a therapeutic enhancement of facial contour in a painless and  
324 non-invasive manner.

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## REFERENCE

- 331 1. Zouboulis CC, Ganceviciene R, Liakou AI, Theodoridis A, Elewa R,  
332 Makrantonaki E. Aesthetic aspects of skin aging, prevention, and local treatment.  
333 Clin Dermatol [Internet]. 2019;37(4):365–72. Available from:  
334 <https://doi.org/10.1016/j.clindermatol.2019.04.002>
- 335 2. Friedman O. Changes associated with the aging face. *Facial Plast Surg Clin*  
336 *North Am.* 2005;13(3):371–80.
- 337 3. Jiang X, Savchenko O, Li Y, Qi S, Yang T, Zhang W, et al. A Review of Low-  
338 Intensity Pulsed Ultrasound for Therapeutic Applications. *IEEE Trans Biomed*  
339 *Eng.* 2019;66(10):2704–18.
- 340 4. Jones IT, Guiha I, Goldman MP, Wu DC. A randomized evaluator-blinded trial  
341 comparing subsurface monopolar radiofrequency with microfocused ultrasound  
342 for lifting and tightening of the neck. *Dermatologic Surg.* 2017;43(12):1441–7.
- 343 5. O'Brien WD. Ultrasound-biophysics mechanisms. *Prog Biophys Mol Biol.*  
344 2007;93(1–3):212–55.
- 345 6. Alhaddad M, Wu DC, Bolton J, Wilson MJ, Jones IT, Boen M, et al. A  
346 Randomized, Split-Face, Evaluator-Blind Clinical Trial Comparing Monopolar  
347 Radiofrequency Versus Microfocused Ultrasound With Visualization for Lifting  
348 and Tightening of the Face and Upper Neck. *Dermatologic Surg.*  
349 2019;45(1):131–9.
- 350 7. Contini M, Hollander MHJ, Vissink A, Schepers RH, Jansma J, Schortinghuis J.  
351 A Systematic Review of the Efficacy of Microfocused Ultrasound for Facial Skin  
352 Tightening. *Int J Environ Res Public Health.* 2023;20(2).
- 353 8. Friedman O, Isman G, Koren A, Shoshany H, Sprecher E, Artzi O. Intense  
354 focused ultrasound for neck and lower face skin tightening a prospective study. *J*  
355 *Cosmet Dermatol.* 2020;19(4):850–4.
- 356 9. Gliklich RE, White WM, Slayton MH, Barthe PG, Makin IRS. Clinical pilot  
357 study of intense ultrasound therapy to deep dermal facial skin and subcutaneous  
358 tissues. *Arch Facial Plast Surg.* 2007;9(2):88–95.
- 359 10. Suh DH, Shin MK, Lee SJ, Rho JH, Lee MH, Kim NI, et al. Intense focused  
360 ultrasound tightening in asian skin: Clinical and pathologic Results: Clinical.  
361 *Dermatologic Surg.* 2011;37(11):1595–602.
- 362 11. Kwack MH, Lee WJ. Efficacy of a home-used high-intensity focused ultrasound  
363 device on wrinkle reduction. *Ski Res Technol.* 2023;29(1):1–6.
- 364 12. Lee JC, Tsoi A, Kornfeld GD, Dawes IW. Cellular responses to.  
365 2013;13(1978):618–34.
- 366 13. Robson MC. Growth factors as wound healing agents. *Curr Opin Biotechnol.*

- 367 1991;2(6):863–7.
- 368 14. Velnar T, Bailey T, Smrkolj V. The wound healing process: An overview of the  
369 cellular and molecular mechanisms. *J Int Med Res.* 2009;37(5):1528–42.
- 370 15. Vachiramon V, Namasondhi A, Anuntrangsee T, Kositkuljorn C,  
371 Jurairattanaporn N. A study of combined microfocused ultrasound and  
372 hyaluronic acid dermal filler in the treatment of enlarged facial pores in Asians. *J*  
373 *Cosmet Dermatol.* 2021;20(11):3467–74.
- 374 16. Vachiramon V, Triyangkulsri K, Iamsumang W, Chayavichitsilp P. Efficacy and  
375 Safety of Microfocused Ultrasound With Visualization in Abdominal Skin  
376 Laxity: A Randomized, Comparative Study. *Lasers Surg Med.* 2020;52(9):831–6.
- 377 17. Friedmann DP. Cryolipolysis for Noninvasive Contouring of the Periumbilical  
378 Abdomen with a Nonvacuum Conformable- Surface Applicator. *Dermatologic*  
379 *Surg.* 2019;45(9):1185–90.
- 380 18. Oni G, Hoxworth R, Teotia S, Brown S, Kenkel JM. Evaluation of a  
381 microfocused ultrasound system for improving skin laxity and tightening in the  
382 lower face. *Aesthet Surg J.* 2014;34(7):1099–110.
- 383 19. Kim Y, Yu H, An S, Ha D, Jung B. Handheld microfocused ultrasound device for  
384 facial lifting: A preliminary study of ULTIGHT. *J Cosmet Dermatol.*  
385 2023;22(11):2982–8.
- 386 20. Alam M, White LE, Martin N, Witherspoon J, Yoo S, West DP. Ultrasound  
387 tightening of facial and neck skin: A rater-blinded prospective cohort study. *J Am*  
388 *Acad Dermatol* [Internet]. 2010;62(2):262–9. Available from:  
389 <http://dx.doi.org/10.1016/j.jaad.2009.06.039>
- 390 21. Ghassemi A, Prescher A, Riediger D, Axer H. Anatomy of the SMAS Revisited.  
391 *Aesthetic Plast Surg.* 2003;27(4):258–64.
- 392 22. White WM, Makin IRS, Barthe PG, Slayton MH, Gliklich RE. Selective creation  
393 of thermal injury zones in the superficial musculoaponeurotic system using  
394 intense ultrasound therapy: A new target for noninvasive facial rejuvenation.  
395 *Arch Facial Plast Surg.* 2007;9(1):22–9.
- 396 23. Laubach HJ, Makin IRS, Barthe PG, Slayton MH, Manstein D. Intense focused  
397 ultrasound: Evaluation of a new treatment modality for precise microcoagulation  
398 within the skin. *Dermatologic Surg.* 2008;34(5):727–34.
- 399 24. Ko EJ, Hong JY, Kwon TR, Choi EJ, Jang YJ, Choi SY, et al. Efficacy and  
400 safety of non-invasive body tightening with high-intensity focused ultrasound  
401 (HIFU). *Ski Res Technol.* 2017;23(4):558–62.
- 402 25. Hantash BM, Renton B, Laurence Berkowitz R, Stridde BC, Newman J. Pilot  
403 clinical study of a novel minimally invasive bipolar microneedle radiofrequency  
404 device. *Lasers Surg Med.* 2009;41(2):87–95.

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