

1 Time-Dependent Fit Adaptation of Two Aligner Materials: A Scanning 2 Electron Microscopy Study

3 Abstract

4 **Background:** The goal of the study is to analyze and differentiate the changes in adaptation
5 of aligner at attachment along with time of two different aligner materials after intra-oral
6 usage: Polyethylene terephthalate-Glycol and Co-polyester.

7 **Materials and methods:** A total of 20 aligner appliances (N=20) were studied, comprising OF
8 10 Polyethylene Terephthalate Glycol (PET-G) aligners and 10 Co-polyester aligners. These
9 aligners were evaluated at two time points: just before use (T₀) and after 15 days (T₁₅) of
10 intraoral usage. Each aligner was used for a 15-day period and then adapted to its
11 corresponding 3D-printed resin model. The aligners were sectioned bucco-lingually at the
12 ellipsoid attachment area, and five samples per material per time point (n = 5) were analyzed.
13 Scanning Electron Microscopy (SEM) was employed to measure gap width changes at five
14 distinct levels within the attachment region. The mean values of gap width changes were
15 statistically analyzed to compare the fit between PET-G and Co-polyester aligners.

16 **Results:** Statistically significant differences (P < 0.005) in fit of aligner were observed at
17 given time points: co-polyester exhibited the smallest gap at T₀, while PET-G showed the
18 largest. Likewise, at various attachment levels, significant differences were found at T₁₅ with
19 the smallest gaps occurring at all the levels except at incisal and gingival end of ellipsoid
20 attachment.

21 **Conclusion:** Co-polyester showed superior properties in the initial and final fit of the aligner
22 than that of PET-G. More dimensional changes were observed in PET-G when compared to
23 Co-polyester due to which non uniform change in gap width is seen after intra-oral usage.

24 **Keywords:**

25 Attachment, adaptational fit, co-polyester, gap width, polyethylene terephthalate-glycol.
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28 INTRODUCTION

29 Clear aligner therapy (CAT) is increasingly recognized as a key treatment option in
30 orthodontics, particularly for adult patients¹. These aligners are crafted from thermoplastic
31 materials, such as polyurethane, polyurethane terephthalate-glycol, polyethylene terephthalate
32 copolyester etc and involves a series of personalized, removable set of aligners designed to

33 gradually shift the teeth based on a precise treatment plan created using advanced 3D imaging
34 software. Recent advancements in attachment designs, materials, and auxiliary devices have
35 greatly improved the biomechanics and reliability of treatment outcomes^{2,3,4}. Research shows
36 that clear aligners can effectively manage various orthodontic issues, including crowding⁵,
37 proclination⁶, distalization⁷, open bite and deep bite⁸. However, more complex cases involving
38 deep bites, rotations, and torque adjustments require careful planning and effective anchorage
39 for successful treatment. The material composition of clear aligners is a critical factor in
40 assessing their effectiveness for predictable outcomes. Clear aligners are primarily made from
41 materials, which may exhibit aging changes within the oral environment. Furthermore,
42 achieving the desired tooth movement depends significantly on the aligner's fit on both the
43 anchorage unit and the teeth involved in the treatment.^{9,10,11}

44 In orthodontics, thermoplastic appliances have a longstanding legacy, and aligner therapy has
45 more recently gained traction as a compelling option across a variety of clinical scenarios.
46 Contemporary studies underscore that aligners offer not only superior aesthetics but also
47 reliable effectiveness in aligning and straightening dental arches, often matching the
48 outcomes achieved by fixed orthodontic devices. Innovations in aligner materials, force
49 delivery systems, and the sequence of tooth correction have substantially improved in treating
50 complex malocclusions enhancing predictability and precision.¹²

51 Clear aligners require consistent full-time wear to facilitate effective tooth movement.
52 Initially, a minimum of 22 hours per day for two weeks was recommended, but this duration
53 often led to patient fatigue and compliance issues, resulting in suboptimal outcomes. As a
54 result, strategies to improve compliance and make treatment more manageable have become
55 a focus in orthodontics.^{3,13,14}

56 This study concentrates on analyzing the fit of aligners on teeth and to investigate any
57 differences in fit between two distinct aligner materials. By assessing these factors, we hope
58 to contribute valuable insights into the effectiveness and clinical application of different
59 aligner technologies in orthodontic practice.

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66 **AIM OF THE STUDY**

67 This study aims to investigate how two different aligner materials affect the adaptation of
68 aligner fit over time at the attachment site, comparing measurements before and after
69 intraoral use.

70 **MATERIALS AND METHODS.**

71 Materials

72 PET-G- 1mm thickness

73 Co-polyester- 1 mm thickness

74 Both these materials have been compared in this study.

75 Armamentarium

76 1. Panda intraoral scanner Freqty Technology

77 2. Phrozen 4K 3D printer

78 3. Chennai Metco BAINCUT LSS cutting machine

79 4. Biostar thermoforming machine

80 5. Scanning electron microscopy setup with JSM IT 300 SOFTWARE

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82 **Study Design**

83 This ex vivo experimental study aimed to evaluate the adaptational fit of two aligner
84 materials—Polyethylene Terephthalate Glycol (PETG) and Copolyester—before and after
85 intraoral usage. The null hypothesis proposed that there would be no statistically significant
86 difference in aligner–attachment fit between the two materials or over time.

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88 **Sample Distribution**

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90 A total of 20 aligner appliances were evaluated, comprising 10 PETG and 10 Copolyester
91 samples. Each material was studied at two time points: before intraoral use (T_0) and
92 immediately after 15 days of wear (T_{15}). Thus, each group consisted of five aligners ($n = 5$
93 per condition; total $N = 20$).

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95 **Sample Preparation and Clinical Procedure**

96 STL files were generated from intraoral scans of a patient with Class I malocclusion requiring
97 minimal tooth movement, such as cases of mild spacing obtained using the Panda Scanner
98 (Fregty Technology). Accompanying records included digital photographs,
99 orthopantomograms, and lateral cephalometric radiographs. Virtual setups were designed
100 under the supervision of an experienced clear aligner specialist to ensure uniformity across
101 both materials.

102 A total of 20 resin models were 3D-printed from the STL files using a Phrozen printer (Fig.
103 1) and thoroughly cleaned prior to use. Ten models were allocated into 2 groups(group-A and
104 group-B). Group-A is thermoformed with PET-G material and group-B thermoformed with
105 co-polyester aligner sheets. Group-A is again sub-divided into group-Ia and group-Ib likewise
106 group-B is subdivided into group-IIa and group-IIb. Where Ia and IIa are used for analysing
107 gap width at T₀ time point and Ib and IIb are used for analysing gap width at T₁₅ time point.

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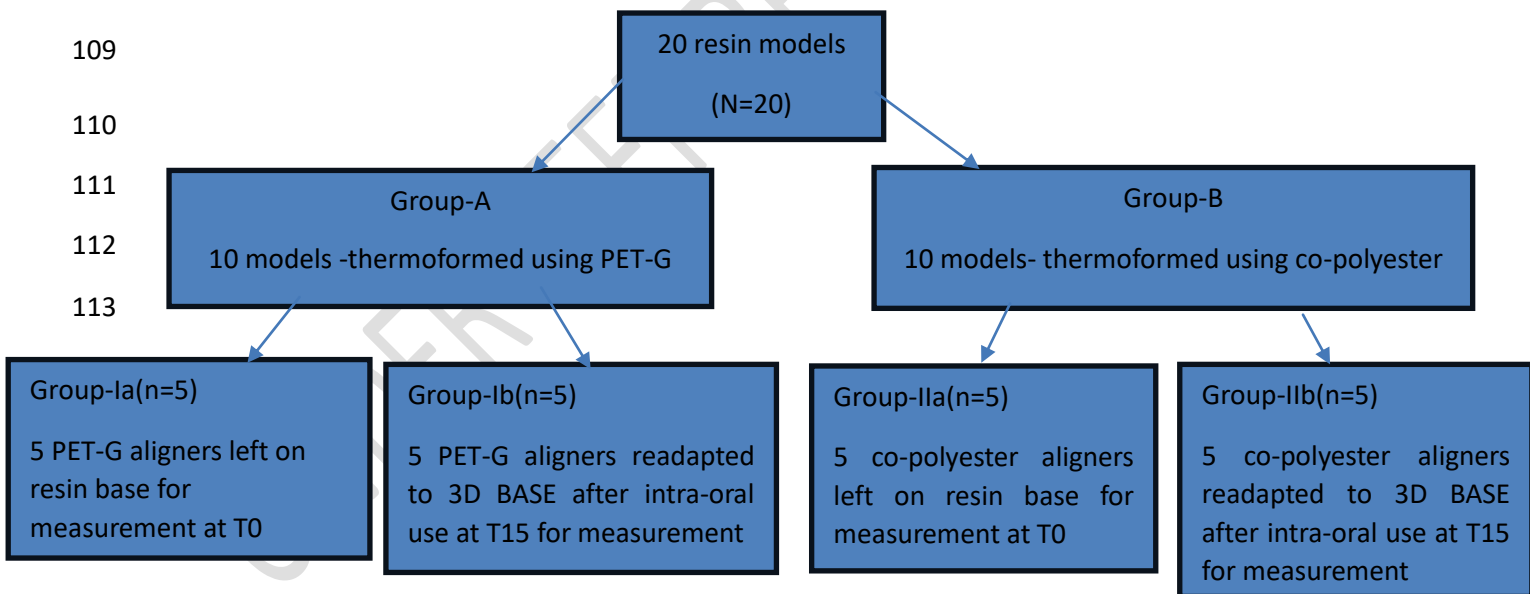
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120 Initial aligners were designed without active force application to minimize shape distortion
121 and were fitted onto the corresponding resin models (Fig. 2). Each model was mounted on an

122 aluminum stub and sectioned labio-lingually through the central incisor region containing an
123 ellipsoid attachment using a low-speed cutting machine (BAINCUT LSS, Chennai Metco)
124 under continuous water irrigation to prevent thermal distortion (Fig. 3).

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126 **Scanning Electron Microscopy (SEM)**

127 Sectioned samples were oriented perpendicular to the long axis of the central incisors. To
128 minimize electrostatic charging and enhance image clarity, each specimen was sputter-coated
129 with a 10 nm layer of 99% pure gold using a Cressington 208HR High-Resolution Sputter
130 Coater (Watford, UK) (Fig. 4). Imaging was performed using a JSM IT 300 high-
131 performance SEM (JEOL, Japan) (fig. 5) equipped with an energy-dispersive X-ray (EDX)
132 analyzer, operated at 15 kV accelerating voltage and 10 mm working distance, with a
133 resolution of 3.0 nm. Representative micrographs were obtained at 500 μm magnification
134 (Fig. 6).

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136 **Measurement Protocol**

137 Micrometric measurements were taken using the JSM IT 300 SEM software on
138 buccolingually sectioned micrographs. Adaptational changes in aligner fit, specifically the
139 microscopic gap between the aligner and the ellipsoid attachment, were monitored at various
140 attachment levels and time intervals (T_0 and T_{15}). A total of fifty measurements at the
141 micrometer level were collected and subjected to analysis, providing a comprehensive
142 assessment of the distances at each specified level.

143 As shown in figure 7., Level 1 represents Incisal end of the attachment, level 2 as
144 Incisal 1/4th of the attachment, level 3 as Labial middle of the attachment, level 4 as Gingival
145 1/4th of the attachment, level 5 as Gingival end of the attachment.

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148 ***Statistical Analysis***

149 For statistical analysis, the data entered into a Microsoft Excel spreadsheet were analysed
150 using IBM SPSS software version 25. The Mann-Whitney U test was applied for inter-group

151 comparisons. A p-value of less than 0.05 was considered statistically significant for all
152 analyses.

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156 **RESULTS**

157 Table 1 and Graph 1 show the changes in mean aligner fit at different levels of the attachment
158 in the PET-Ggroup from T₀ to T₁₅. The fit at the incisal end decreased from 419.42 to 397.20,
159 and at the incisal one-fourth, it dropped from 345.58 to 313.24. A more significant reduction
160 was seen at the middle of the attachment, where the fit fell from 261.98 to 10.60. In contrast,
161 the gingival one-fourth rose from 334.18 to 567.28 and the gingival end showed an increase
162 from 99.60 to 413.84. All these changes were statistically significant, with p-values ranging
163 from 0.041 to 0.043.

164 Table 2 and Graph 2 show the intra-group comparison of mean aligner fit at different levels
165 of the attachment in the Co-polyestergroup from T₀ to T₁₅. At the incisal end, the mean fit
166 increased from 274.30 to 623.80, and at the incisal one-fourth, it rose from 144.52 to 276.00.
167 The middle of the attachment also showed an increase from 64.82 to 130.36, while that the
168 gingival one-fourth, the fit showed only a slight increase from 223.14 to 223.18, which was
169 not statistically significant ($p = 0.50$). However, gingival end improved from 19.56 to 113.90.
170 All these changes were statistically significant, with p-values ranging from 0.041 to 0.043.

171 Table 3 and Graph 3 show the inter-group comparison of mean aligner fit at different levels of
172 the attachment at T₀. At the incisal end, the co-polyester group had a higher mean fit(274.30)
173 compared to the PET-G group(419.42), which was statistically significant ($p = 0.009$).
174 Similarly, at the incisal one-fourth, the mean fit was 345.58 in the PET-Ggroup and 144.52 in
175 the Co-polyestergroup ($p = 0.010$). At the middle of the attachment, the PET-Ggroup showed
176 a mean of 261.98, significantly greater than the Co-polyestergroup's 64.82 ($p = 0.009$). At the
177 gingival one-fourth region, the copolyester group demonstrated a significantly higher mean
178 fit (223.14) compared to theCo-polyestergroup (334.18) ($p = 0.010$). Additionally,gingival
179 margin the PET-Ggroup exhibited a mean fit of 99.60, whereas the Co-polyestergroup
180 showed a mean fit of 19.56 ($p = 0.009$).

181 Table 4 and Graph 4 present the inter-group comparison of mean aligner fit at different levels
182 of the attachment at T_{15} . At the incisal end, the Co-polyester group showed a higher mean
183 fit (397.20) compared to the PET-G group (623.80), which was statistically significant ($p =$
184 0.008). At the incisal one-fourth, the co-polyester had a slightly higher fit (276.00) than the
185 PET-G group (313.24), also statistically significant ($p = 0.009$). In the middle of the
186 attachment, the PET-G group had a greater mean fit (10.60) compared to the PET-
187 G group (130.36) ($p = 0.009$). At the gingival one-fourth, the co-polyester group again showed
188 a higher fit (223.18) compared to the PET-G group (567.28), which was statistically significant
189 ($p = 0.009$). Lastly, gingival end, the co-polyester group (113.90) had a much higher fit than
190 the PET-G group (413.80), with a significant difference ($p = 0.007$).

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192 **DISCUSSION**

193 This study aims to investigate how two different aligner materials affect the adaptation of
194 aligner fit over time at the attachment site, comparing measurements before and after
195 intraoral use. The attachment on the model is ellipsoid which is most commonly used for
196 space closure. Multiple factors must be considered when evaluating the efficiency and
197 effectiveness of aligners^{15,16}. According to Fang et al., the mechanical characteristics of
198 thermoplastic materials showed no statistically or clinically significant changes after intraoral
199 use¹⁷. Gaining insight into the biomechanical force dynamics between aligners and
200 attachments is key to enhancing aligner performance. The type of interaction whether passive
201 or active, significantly influences treatment outcomes. Fry et al. conducted a clinical trial with
202 10 moderately complex cases to evaluate the effectiveness of three different aligner change
203 protocols for 2 weeks and 1 week combined with AcceleDent. After 12 weeks, all groups
204 demonstrated comparable aligner fit, indicating that, in the short term, the frequency of
205 aligner changes may not significantly influence fit¹⁸. Conversely, Linjawi et al. (2022)
206 demonstrated that a 15-day wear period resulted in better adaptation and the least width
207 between the attachment and aligner, as observed through scanning electron microscopy
208 (SEM)¹. Their study showed that while width remained relatively consistent across days 3, 7,
209 and 10, it varied depending on the location of attachment.

210 **Comparison of Initial Fit (T_0)**

211 At baseline (T_0), the Co-polyester aligners exhibited a smaller mean gap width across most
212 attachment levels compared to the PET-G aligners indicating a superior initial fit. This could

213 be attributed to the inherent material properties of Co-polyester including higher rigidity and
214 better thermoforming accuracy, which allow closer adaptation to the attachment surfaces.
215 PET-G by contrast, possesses greater elasticity and lower form stability upon thermoforming
216 which may result in slightly increased internal stress relaxation and dimensional deviations
217 following fabrication.
218 These findings align with previous studies suggesting that Co-polyester-based aligners
219 demonstrate enhanced mechanical strength and better reproduction of fine surface details
220 following thermoforming compared to PET-G-based materials^{19,20}. The superior adaptation of
221 Co-polyester at T0 thus supports its suitability for applications requiring precise attachment
222 engagement and effective force transmission during the early phase of treatment.

223 **Effect of Intraoral Usage (T₁₅)**

224 After 15 days of intraoral usage (T₁₅), both materials exhibited notable alterations in fit,
225 though the direction and magnitude of changes differed between groups. PET-G aligners
226 demonstrated a nonuniform variation in gap width, with a reduction in fit at the incisal and
227 middle levels but an increase at the gingival ends. This irregular pattern suggests localized
228 deformation and potential relaxation of the material due to cyclic thermal and mechanical
229 stresses encountered intraorally such as temperature fluctuations, salivary moisture
230 absorption, and masticatory forces.

231 Conversely, Co-polyester aligners exhibited more uniform dimensional changes with a
232 general increase in gap width across most attachment levels. Although the increase indicates
233 slight expansion or stress relaxation, the extent of change was smaller and more consistent
234 compared to PET-G. The superior dimensional stability of Co-polyester could be related to its
235 higher glass transition temperature (T_g) and reduced water absorption rate, which minimize
236 distortion during wear. These results corroborate previous investigations that highlighted Co-
237 polyester's improved resistance to deformation under oral conditions^{10,21}.

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240 **LIMITATIONS**

- 241 • The repeatability of micrometric measurements has not been done.
- 242 • Smaller sample size.

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CONCLUSION

- ❖ The PET-G aligners showed a significant decrease in fit at the incisal and middle regions from T_0 to T_{15} , while the gingival regions exhibited a marked increase in fit, indicating material deformation or relaxation leading to differential adaptation over time.
- ❖ The co-polyester aligners demonstrated a significant improvement in fit at most attachment levels over the 15-day period, suggesting better dimensional stability and consistent adaptation, except at the gingival one-fourth where the change was not significant.
- ❖ At T_0 , the co-polyester aligners exhibited superior fit compared to the PET-G aligners at all attachment levels, indicating better initial adaptation of the co-polyester material immediately after fabrication.
- ❖ By Day 15, PET-G aligners showed higher fit values in the incisal and middle regions, while co-polyester aligners maintained better fit at the gingival areas, reflecting material-dependent changes in aligner adaptation over time.

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